

Determining Disease Evolution Driver Nodes in Dementia Networks

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Determining the Most Influential Nodes in Pinning **Controllability of Connectivity Networks**

Results



Node





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Figure: Schematic illustration of unweighted-undirected graph of complex networks in brain. Nodes or vertices can be brain regions or voxels. Edges or links are the functional or structural connections between nodes.

We consider an undirected and unweighted network (V,E) with the set of N nodes (or vertices) \mathbf{V} and a set of edges \mathbf{E} . Each node is assumed to be a dynamical system with the following dynamical equation:

$$\frac{dx_i}{dt} = F(x_i) - \sigma \sum_{j=1}^{N} l_{ij} H x_j$$
(1)

where $x_i \in R_n$ is the **n**-dimensional state vector, $F : R_n \to R_n$ defines the indi-



(b) Functional

(a) Structural

Figure: The most influential driver nodes (shown in red) in connectivity graphs for (a) CN, (b) MCI and (c) AD.

Conclusion

vidual systems dynamical equation, which is considered identical for all nodes in this paper, and σ represents unified coupling strength. $L = [l_{ij}] = D - A$ is the Laplacian matrix of the graph (V,E), where A is the adjacency matrix and \mathbf{D} is a diagonal matrix of nodes degrees. Non-zero elements of \mathbf{H} determine the coupled elements of the oscillators. The pinning control objective is to synchronize all nodes to the following desired state (i.e. $x_1(t) = x_2(t) = \cdots = x_N(t) = s(t)$):

$$\frac{l(s(t))}{dt} = F(s(t)) \tag{2}$$

In order to pin the dynamical network [1, 2, 3] to this reference, the following control system should be designed:

$$\frac{dx_i}{dt} = F(x_i) - \sigma \sum_{j=i}^{N} l_{ij} H x_j + \beta_i u_i \qquad i = 1, 2, 3, \cdots, N \qquad (3)$$

where u_i is the control signal and $\beta_i = 1$ for driver nodes, otherwise $\beta_i = 0$. The system can be linearized over an equilibrium point x_e as follows:

$$\frac{dz_i}{dt} = [DF(x_e) - \sigma\lambda_i H]z_i + \beta_i u_i \qquad i = 1, 2, 3, \cdots, N \qquad (4)$$

Data indicate that the connections in the structural graphs illustrate the interregional covariation of gray matter volumes in different areas. The connections in the functional graphs do not illustrate the correlation in activity. However, they show the correlation in the glucose uptake between different regions.

References

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where **D** stands for the Jacobian, λ_i is the i^{th} eigenvalue of the Laplacian matrix of the graph. In order to find the node with the most influence on pinning controllability, we restate the following definition and lemma [4].

Definition: For each node i of the undirected network (V,E), the Eigenratio Sensitivity Index **(ESI)** is defined as:

$$ESI(i) = [x_N^i]^2 \tag{5}$$

where x_N^i represents the *i*th element of x_N , the eigenvector corresponds to the largest eigenvalue of the Laplacian matrix (λ_N) .

We apply the theoretical results on functional (18 FDG-PET) and structural (MRI) connectivity graphs for CN, MCI, and AD patients. These data were obtained from the Alzheimer's Disease Neuroimaging Initiative (ADNI) database. For the structural MRI data, the connections in the graph show the inter-regional covariation of gray matter volumes in different areas while for the functional PET data, the connections do not show the correlation in activity.

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